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(54) **HIGH FREQUENCY ALTERNATING CURRENT MEDICAL DEVICE WITH SELF-LIMITING CONDUCTIVE MATERIAL AND METHOD**

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USPC ..... 606/32-35, 41, 48-50  
See application file for complete search history.

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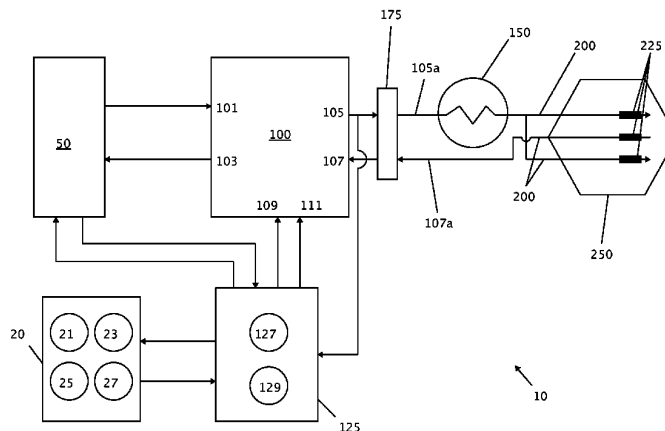
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(57) **ABSTRACT**

A high frequency alternating current medical device and method of using such is disclosed. High frequency alternating current medical device comprises a power source, an electric field generator, a self-limiting conductive material electrical component, at least one probe or needle-type projection, and at least two conductive segments located on probe or needle-type projection. At least two conductive segments are electrically connected to electric field generator so that an electric field is created between conductive segments, which induces an electrical current, which generates heat, and causes a certain desired precise cell injury. Self-limiting conductive material electrical component allows such precise cell injury because it limits electrical current through target tissue. Invention may be used in medical, dental, or veterinary applications. Exemplary embodiments include cosmetic applications, treatment of wrinkles, remodeling of subcutaneous tissue, treatment of muscle spasms, and others. Medical device can be small, hand-held, and easily manipulated to perform surgery.

**24 Claims, 9 Drawing Sheets**



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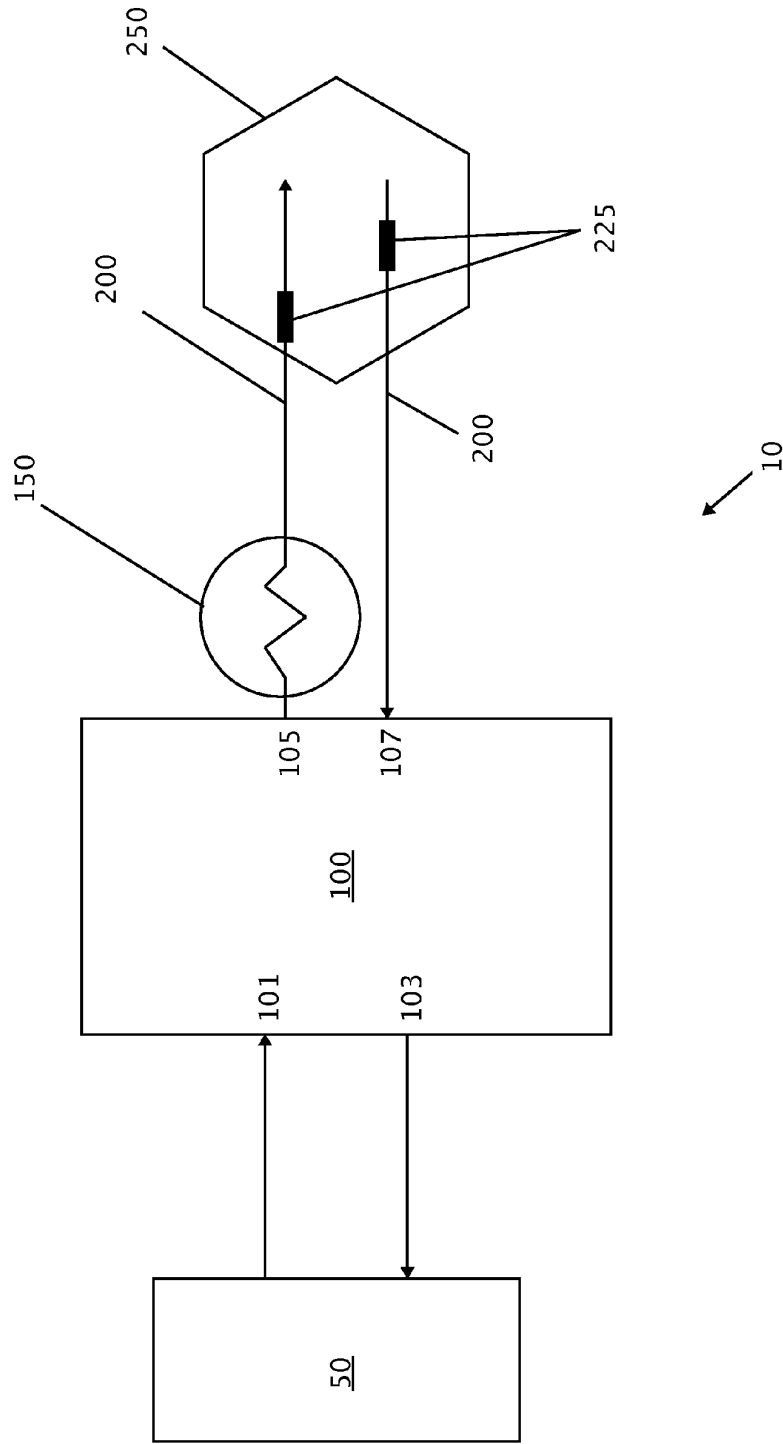


Fig. 1

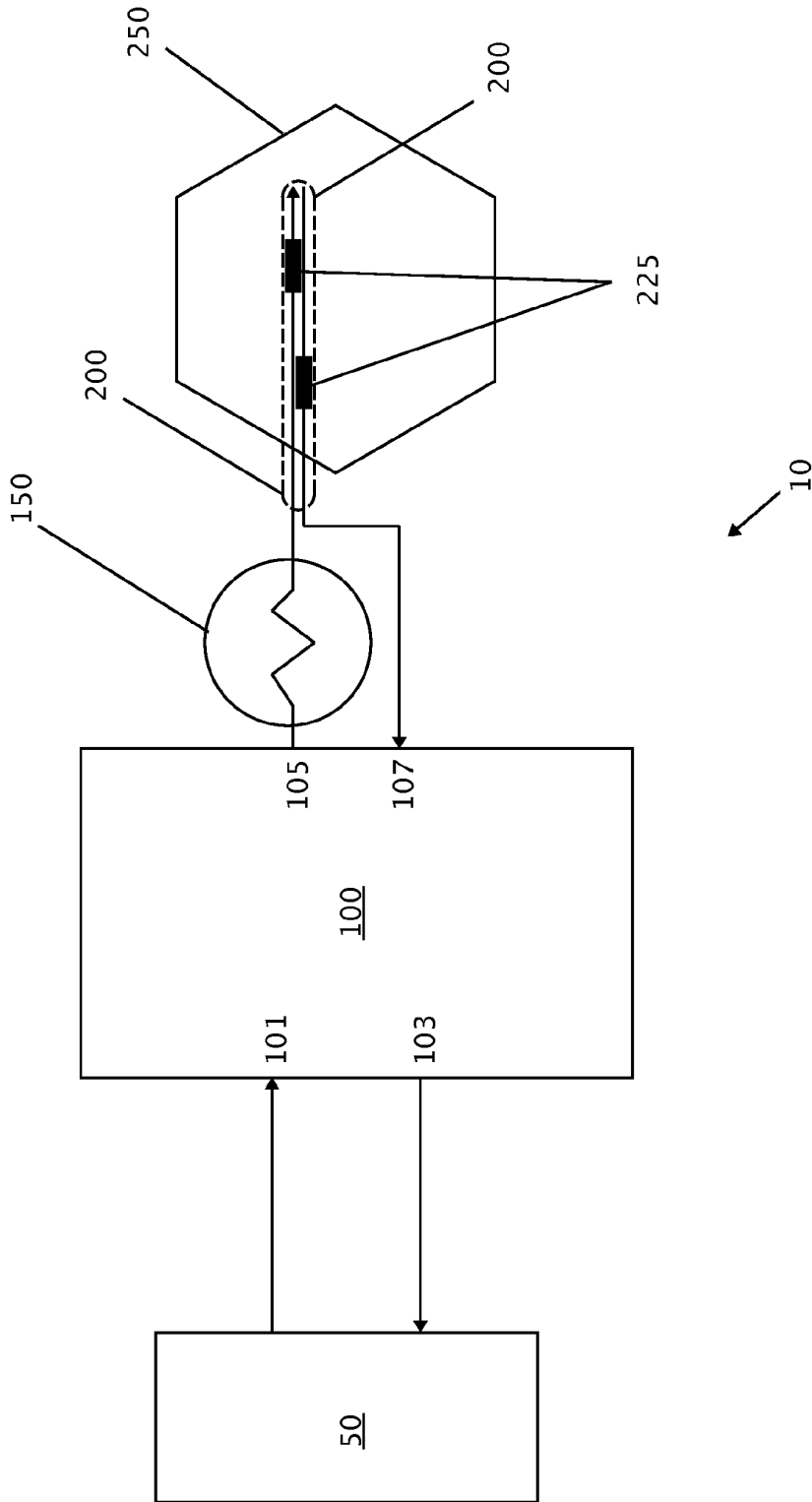


Fig. 1A

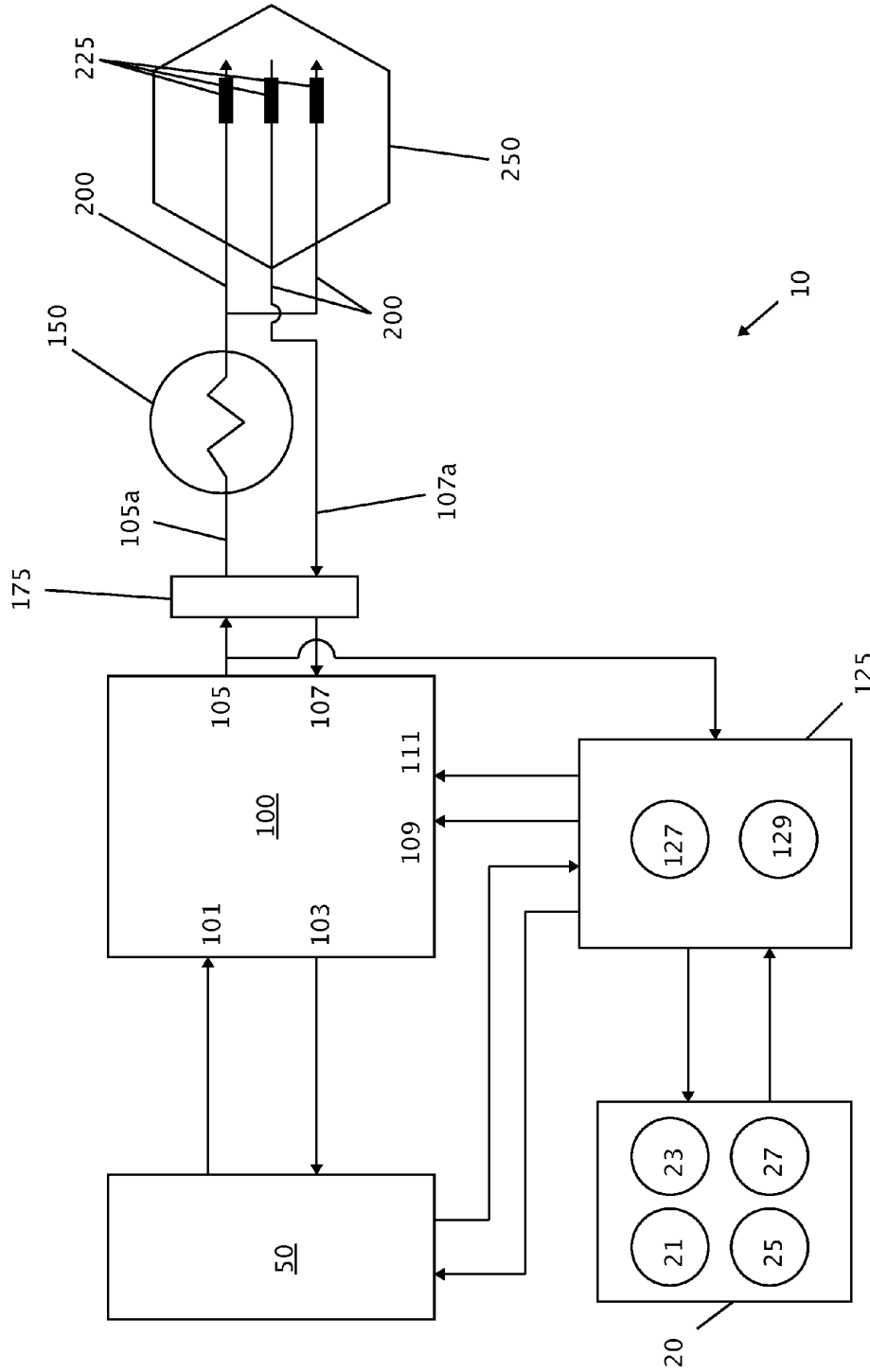


Fig. 2

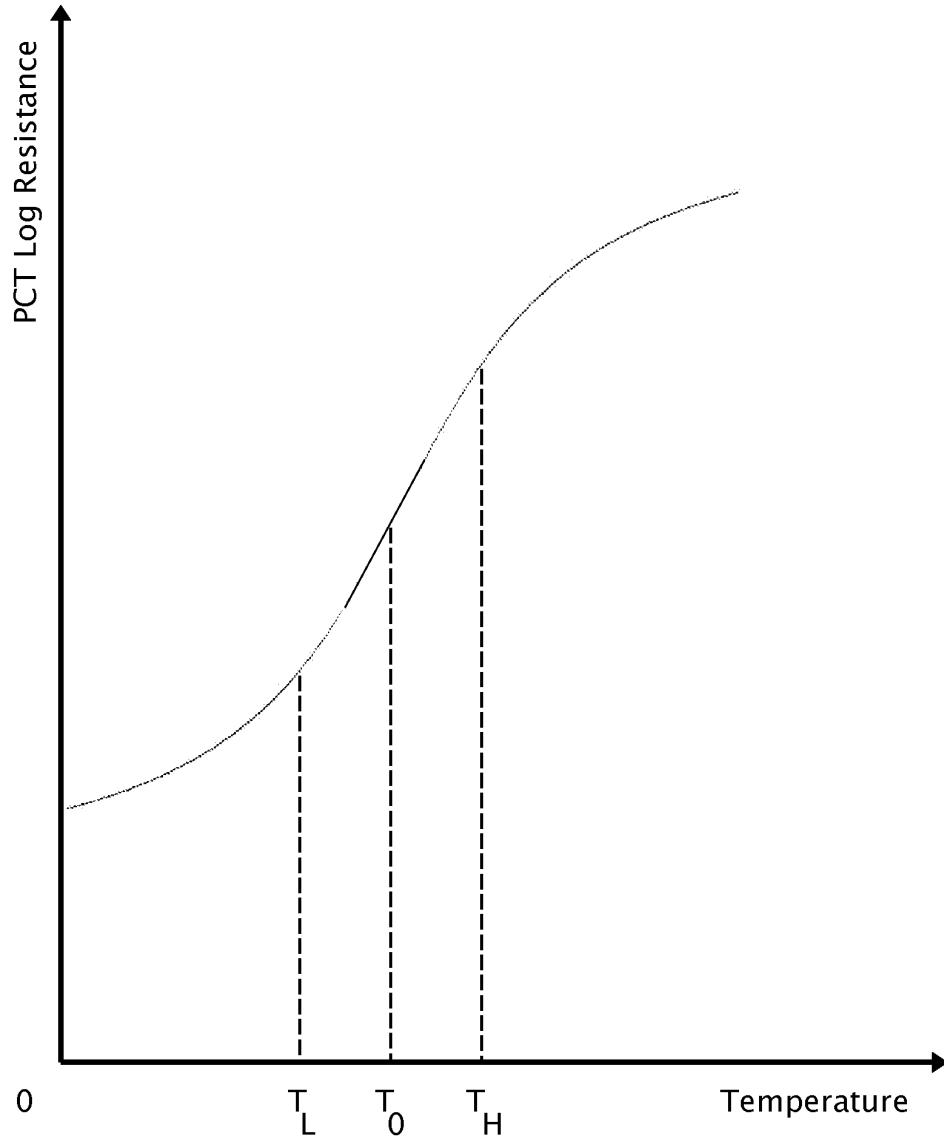


Fig. 3

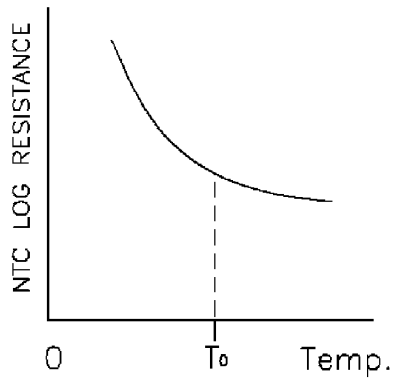


Fig. 4A

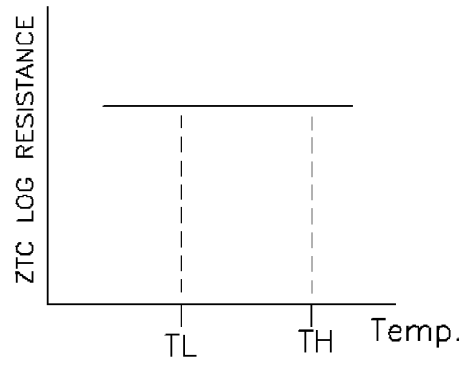


Fig. 4B

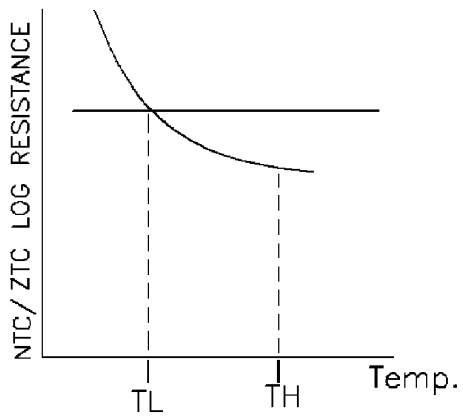


Fig. 4C

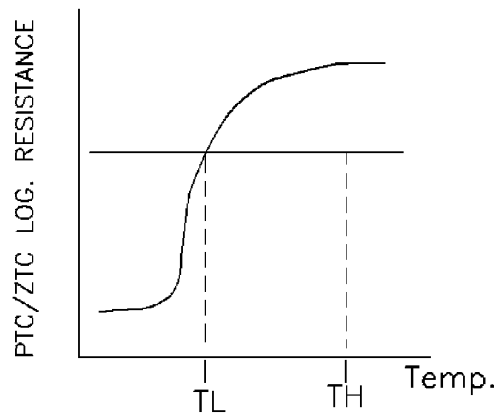


Fig. 4D

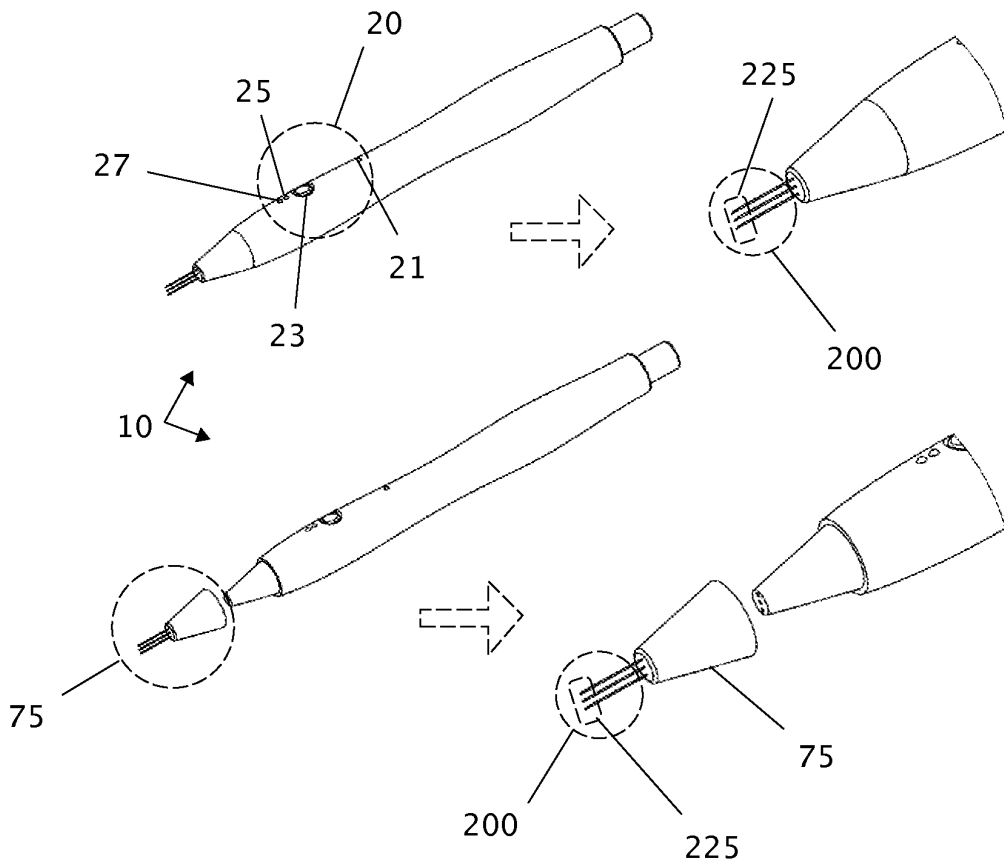


Fig. 5



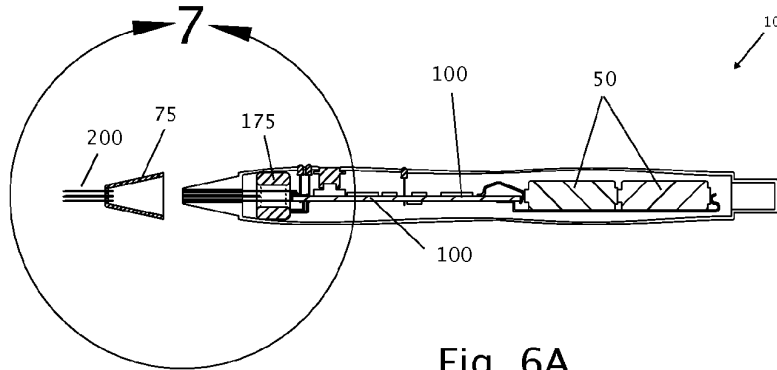


Fig. 6A

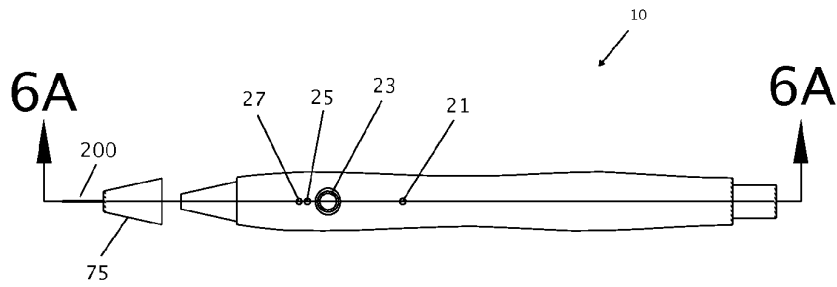


Fig. 6B

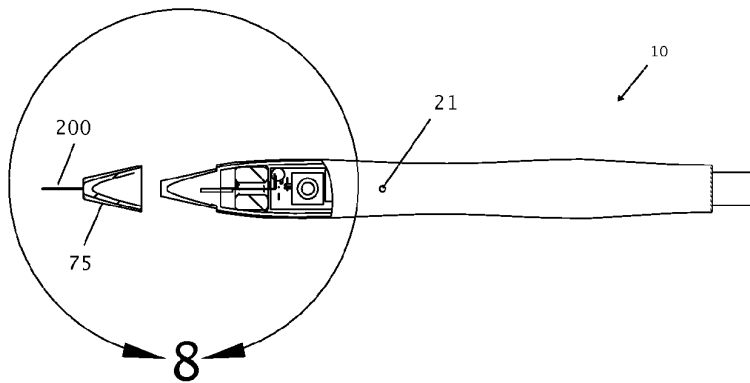


Fig. 6C

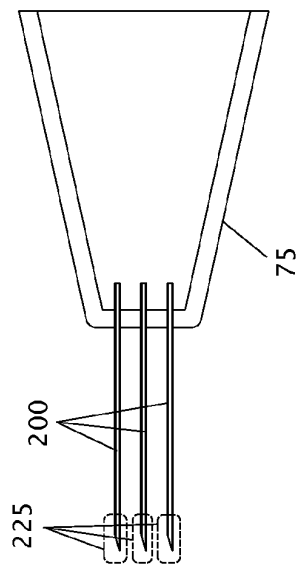
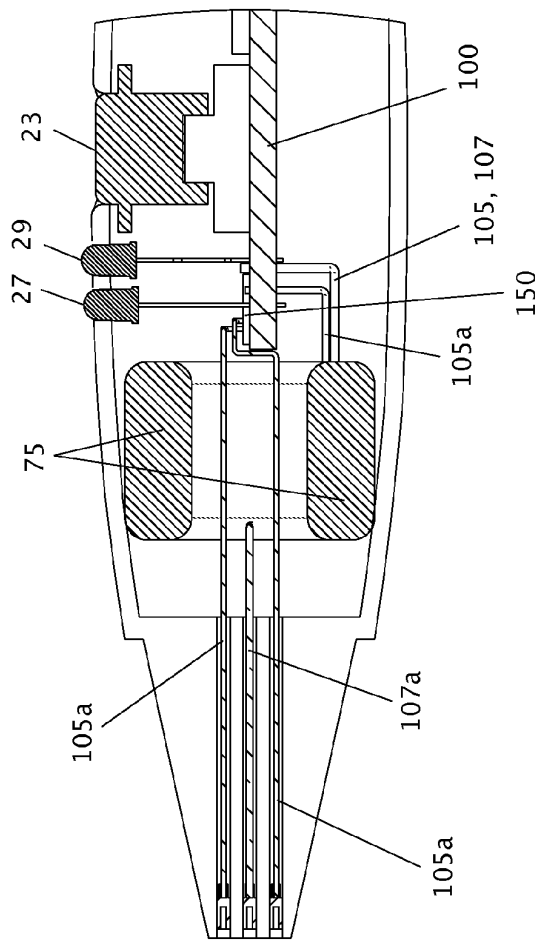


Fig. 7

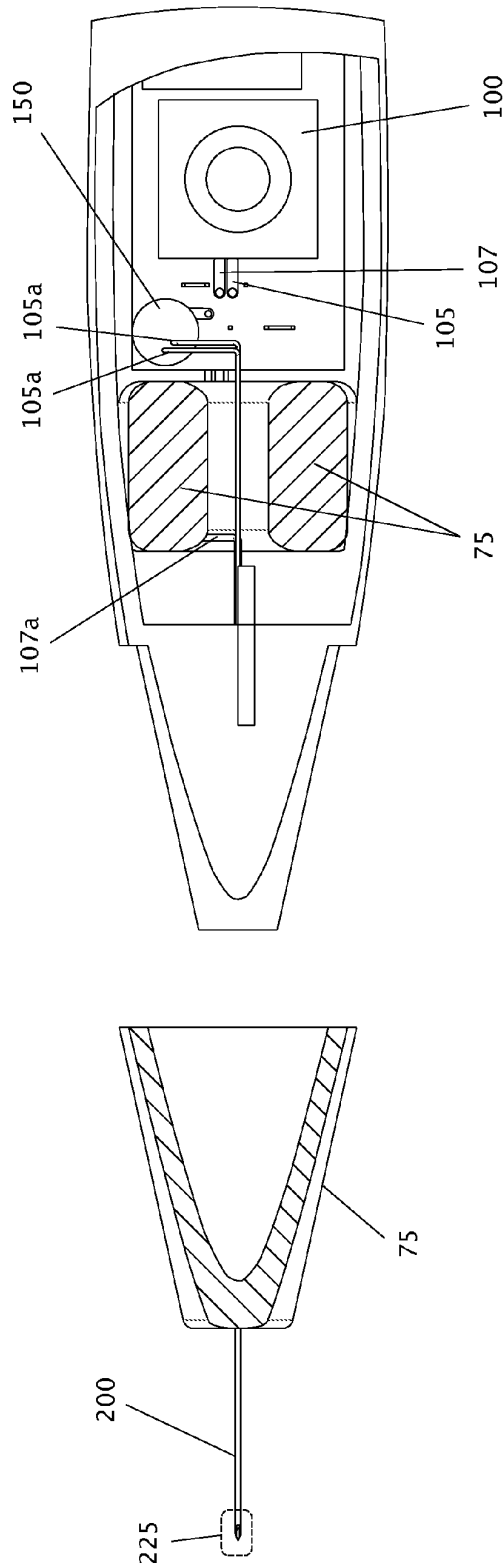


Fig. 8

**HIGH FREQUENCY ALTERNATING  
CURRENT MEDICAL DEVICE WITH  
SELF-LIMITING CONDUCTIVE MATERIAL  
AND METHOD**

BACKGROUND OF THE INVENTION

1. Field of the Invention

This invention relates to electrosurgical devices. Electrosurgery is the application of a high-frequency electric current to tissue as a means to cut, coagulate, desiccate, or fulgurate tissue. Its benefits include the ability to make precise cuts with limited blood loss. Electrosurgery also includes surgical procedures where one or more localized portions of tissue are ablated using high frequency alternating current to generate heat, without heating other types of tissue near the target tissue. Electrosurgery devices use probe-like structures to physically contact the target tissue where such structure is a type of electrode acting to pass electrical current to the tissue. Electrosurgery devices typically cause substantial physical damage to tissue.

This invention applies an electrical field across target tissue, causing an electrical current to “conduct” across said target tissue. Heat is produced from this electrical current by ohmic or joule heating where the heat produced from such is proportional to the square of the amount of this current. A “lesion area” is created where tissue is heated above normal temperature. Heating occurs in a very controlled way where temperature of the lesion area does not rise above a maximum temperature. Carefully controlled heating provides the opportunity to cause a desired precise cell injury. The invention carefully controls heat generation in the lesion area with a self-limiting conductive material electrical component in electrical series connection with the electrical current in the target tissue. Self-limiting conductive material electrical component precisely controls the electrical current flowing across the target tissue.

Electrical current is directly proportional to heat production, which is directly proportional to temperature increase, where elevated temperature and duration of such, along with location and size of the lesion area, primarily determine the type and extent of cell damage, which, in turn, determines whether the desired precise cell injuries are attained. Thus, this invention uses precise current control to yield a precise minimum level of cell injury required to effect the desired result for the patient without going beyond this level, thereby effecting the result without unnecessary cell injury. All prior art electrosurgical devices and radio frequency medical devices cannot control temperature or heat production as precisely as this invention and thus cause more damage to target tissue.

The invention may be used in medical, dental, or veterinary applications. Exemplary embodiments of the invention have cosmetic applications including treatment of wrinkles and remodeling of subcutaneous tissue. Exemplary embodiments are also used for therapeutic applications including treatment of muscle spasms and chronic pain and the control of one or more muscles of other target tissue. Exemplary embodiments are designed to specifically affect nerve tissue where the desired cell injury is to “deaden” the nerve or break the electrochemical connection, either temporarily or permanently, between nerve and muscle that causes nerve-to-muscle contractile function. However, this invention may be used to cause a desired precise cell injury to any type of cell or organ in the body within only the limitation of the relative sizes of the probes/needles on the invention apparatus as manufacturing technology changes with the times as com-

pared to the size of the particular cells of interest, where cells may be of any type known human or otherwise.

2. Description of Related Art

A nerve is a cell that is relatively large. Each nerve cell contains a soma, multiple dendrites, an axon fiber, and multiple axon terminals. The soma is the central part of the nerve; it contains the nucleus of the cell. The soma can range from 4 to 100 micrometers in diameter. The axon and dendrites are filaments that extend outward from the soma. Many dendrites typically surround and branch off from the soma, and have length of up to a few hundred microns. The axon is a single cable-like projection extending outward from the soma that can extend over 100 times the diameter of the soma. The axon carries electrochemical nerve signals away from the soma to effectively control one or more muscles. Axon terminals are located opposite the soma-end of the axon. Typically, axon terminals terminate in a branch network of synapses, which release chemicals to communicate with one or more muscles or other tissue or with other dendrites or soma from another nerve cell within a chain of nerve cells leading to one or more muscles or other tissue.

Typically, a large number of axons from many cells are bundled together in a large conduit called an epineurium, with other nested conduits inside. Analyzing the physiological structure of these conduits, we start with an inner conduit or sheath called an endoneurium, which directly surrounds each axon. Multiple axons are typically grouped together into fascicles and further protected by a mid level sheath called a perineurium. Further, multiple perineurium bundles of axons are typically nested within an outer sheath called an epineurium. This is widely known in the art. Thus, each axon is protected by at least three sheath layers, i.e. an epineurium, a perineurium, and an endoneurium, going from outer most to innermost layer. Note that each large conduit or epineurium contains very many bundles of endoneurium conduits, thus it would be possible to sever completely the axons of some nerve cells, while leaving intact the complete endoneurium of other nerve cells.

This prompts a basic discussion of nerve cell injury. The Seddon system is a basic classification system used to describe nerve injury where there are three categories of injuries—neuropraxia, axonotmesis, and neurotmesis. The following is also well understood in the art.

With neuropraxia, the integrity of the axon is preserved so the endoneurium, perineurium, and epineurium are all intact, but there is an interruption in conduction of the electrochemical impulse traveling down the axon. This is the mildest form of nerve injury. Neuropraxia is typically a biochemical lesion caused by concussion injuries to the cell. There is a temporary loss of function, which is reversible within hours to months of the injury (the average is 6-8 weeks).

With axonotmesis, the integrity of the axon is interrupted but the endoneurium, perineurium, and epineurium are not punctured or deformed significantly. The result is typically loss of both motor and sensory functions, but with recovery through regeneration of the axon, a process that takes place at a certain rate per day, typically taking longer than neuropraxia for recovery. With neuropraxia and axonotmesis the intact endoneurium provides a guide for axonal regeneration where the nerve regenerates along the endoneurial tubules.

Conversely, with neurotmesis, the integrity of the supporting structures are disrupted or punctured, disrupting axonal regrowth and reimplantation. Typically, the injury results from severe contusion, stretch, or laceration of the cell or other internal disruption of the cell architecture sufficient to involve the perturbation of the endoneurium, perineurium, or epineurium. Results are typically complete loss of motor,

sensory, and autonomic function. Thus, the electrochemical signals do not complete the connection to the muscle or target tissue. Neurotmesis injury is typically permanent.

Comparably, a temporary type of neurotmesis results from nerve toxicity caused by local anesthetic, which is typically injected in or near a nerve cell. Anesthetic also disrupts the electrochemical signals sent to the muscle, thereby causing a loss of motor, sensory, and autonomic function. Botulinum toxin or Botox®, as used with the popular cosmetic procedure for wrinkles, is used as a neuromodulator that works at the neuromuscular junction to block the transmission between the nerve and muscle resulting in paralysis of the muscle to reduce wrinkles.

This invention is first to provide the ability to effect a wide range of cell injury from a minimum level of neuropraxia to full neurotmesis, through electrical current heating means, without also effecting large-scale physical damage in the target area. This invention can provide temporary effects or permanent relief to a patient without surface tissue cosmetic defects.

#### BRIEF SUMMARY OF THE INVENTION

The invention comprises a medical device and method of using such. Medical device comprises at least one probe or needle-type projection at its distal end and at least two conductive segments located on said at least one probe or needle-type projection. At least one probe or needle-type projection is capable being inserted into a body cavity or into body tissue, at which point also capable of conducting electrical current between said at least two conductive segments. In “one-probe or needle-type projection” mode, said at least two conductive segments are located on the one and only probe or needle-type projection. In “two-probe or needle-type projection” mode, one of said at least two conductive segments is typically located on each of the two probes or needle-type projections. Probes or needle-type projections are typically inserted into tissue or a body cavity containing the target cells or into nearby to such; then an electrical current is conducted between said segments to effect the desired precise cell injury. Probes or needle-type projections may be inserted into tissue, so that electrical current occurs subcutaneously. In this fashion, the heat-defined lesion area is entirely subcutaneous, resulting in minimal change of appearance on the surface of the tissue.

Medical device further comprises a power source capable of applying the appropriate electrical fields across said at least two conductive segments in order to generate the appropriate electrical current in the target tissue. The power source may be alternating current or direct current.

Best mode medical device further comprises an electric field generator capable of being powered by said power source and generating one or more electric fields across said at least two conductive segments. In best mode, electric field generator is small and miniaturized. Electric fields may be generated in continuous wave form, such as sine, triangular, or square wave or similar, and at various frequencies, intensities, and polarizations in order to yield the exact desired heating to cause the desired precise cell injury. Electric fields may be of a direct current pulse nature, as well, such as sine, triangular, or square wave or similar pulse shape. Electric field generator may emit several different shaped pulses and continuous wave forms at the same time. Electric field generator may be small enough to be handheld but also capable of supplying a 3-watt field into 150 ohms at 460 KHz using a hand-held direct current battery power source.

Medical device further comprises a self-limiting conductive material electrical component in electrical series connection with said electrical current passing through the target tissue. “Self-limiting conductive material” is defined as a material whose electrical resistive properties vary with its temperature. Self-limiting conductive material electrical component functions electrically like a thermistor, a thermocouple, or a switch in the electrical heating circuit of the target tissue. Self-limiting conductor material electrical component, in effect, controls the electrical current passing through the target tissue, and thus controls the temperature of the target tissue, and tissue surrounding target tissue.

Entire medical device may be small enough to be handheld. Power source, electric field generator, self-limiting conductive material electrical component, at least one probe or needle-type projection, and at least two conductive segments may be incorporated into one device, small and light enough to be comfortably held and very effectively handled by the surgeon to perform surgery.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a circuit diagram of a basic mode of medical device with two probes or needle-type projections.

FIG. 1A is a circuit diagram of a basic mode of medical device with one probe or needle type projection.

FIG. 2 is a circuit diagram of best mode of medical device.

FIG. 3 is a logarithmic graph of electrical resistance (ohms) versus temperature (C) for best-mode self-limiting conductive material electrical component, which is a PTC material thermistor.

FIGS. 4A-D depict logarithmic graphs of electrical resistance (ohms) versus temperature (C) of a NTC, a ZTC, a NTC/ZTC layered material, and a PTC/ZTC layered material respectively.

FIG. 5 shows perspective views of best mode medical device with replaceable tip attached and replaceable tip removed, with blow-up views of each.

FIG. 6A is a cross-section of best mode medical device. FIG. 6A also defines the blow-up view of FIG. 7.

FIG. 6B is top plan view of medical device. FIG. 6B also defines cross-sectional plane 6A.

FIG. 6C is a cut-away view of FIG. 6B. FIG. 6C also defines the blow-up view of FIG. 8.

FIG. 7 is a blow-up of a side elevation view of the distal end of medical device.

FIG. 8 is a blow-up of a top plan view of the distal end of medical device.

#### DEFINITION LIST

Main Term	Definition
10	Medical Device
20	User Interface
21	Main Power on/off Switch
23	Electric Field on/off Switch
25	Power Indicator Light
27	Electric Field Indicator Light
50	Power Source
75	Removably Attachable Surgical Tip for Medical Device
100	Electric Field Generator
101	Power Input Positive
103	Power Input Negative
105	At Least One Phase Signal Output
105a	Transformed 105 Signal
107	At Least One Common Signal Output
107a	Transformed 107 Signal

-continued

## DEFINITION LIST

Main Term	Definition
109	Trimmer Input
111	Trimmer Input
125	Control Module
127	Frequency Modulation Control
129	Current Cut-off Setting
150	Self-limiting Conductive Material Electrical Component
175	Transformer
200	At Least One Probe or Needle-type Projection
225	At Least Two Conductive Segments on 200
250	Target Tissue

## DETAILED DESCRIPTION OF THE INVENTION

A power source **50** is required to generate the electric field between a set of at least two conductive segments (conductive segments) **225**. Power source **50** may directly generate the electric field between conductive segments **225** or alternatively power source **50** may indirectly power an electric field generator **100**, which in turn generates the electric field between conductive segments **225**. Power source **50** may be a direct current or an alternating current power source. In the case of a direct current power source **50**, the electric field generator **100** would be required to produce alternating current or alternating polarity electric fields in the target tissue **250**. Best mode power source **50** is a direct current battery because there are many standard sizes of such batteries that are small in size but also capable of powering a special electric field generator device capable of producing the appropriate electric fields resulting in the desired precise cell injury.

Alternating current, as opposed to direct current, is preferred because alternating current can produce more heat per amp than direct current in this situation. There appears to be a particular resonance frequency or spike frequency where heat production is maximized from alternating current travelling across a particular type of target tissue **250**. At this frequency, current passes through the target tissue **250** with the least resistance. Thus, at a particular resonance frequency of a particular target cell, less power is required to produce the same or more heat in that cell. This design is preferred because it reduces the power requirements of the device, and thereby allows the device to be small enough to be hand-held. The resonance frequency of nerve cells and their surrounding tissue is 460 KHz and thus is the best mode frequency. There are prior art electrosurgical devices that operate at this frequency because this frequency appears to be the resonance frequency of many types of tissue, not just nerve tissue.

Electric field generator **100** comprises a pulse width modulation power supply electrically connected to common circuit board components including resistors, capacitors, diodes, and switches. Electric field generator **100** may further comprise a transformer **175**, where the output signals from said pulse width modulation power supply are the primary connections with said transformer. Electric field generator **100** is typically custom designed to generate a specific alternating polarity field, with a specific frequency and power, in order to function properly with the specific probe/extension **200** of device **10** according to the requirements to yield the specific desired precise cell injury. In the case of best mode electric field generator **100**, extensive development was expended to yield an electric field generator **100** that is appropriate for nerve cells using a three-needle probe **200** where the generator was also designed to be of a very small size. Best mode electric

field generator **100** includes said pulse width modulation power supply and circuit board components assembled onto a custom circuit board, of a overall long and narrow shape such as rectangle, that is capable of fitting inside of an enclosure of the shape and size of a typical pen as depicted on FIGS. **5-8**. Alternately, electric field generator **100** may consist of many electrical circuit boards that are electrically connected by loose wires to fit inside of various differently shaped enclosures. Best mode electric field generator **100** includes a doughnut shaped transformer **175** electrically connected to the distal end of said custom circuit board with the distal end inside the doughnut hole of transformer **175**, where the secondary voltage and current from transformer **175** is passed through the target tissue **250**.

Best mode pulse width modulation power supply comprises at least six electrical connections: two power input connections consisting of positive and negative power connections **101** and **103**; two signal output connections **105** and **107**; and two trimmer input connections **109** and **111**. Output signals **105** and **107** create electric fields in the target tissue located between conductive segments **225** in rapidly changing alternating polarity in order to generate or induce the alternating current in the target tissue. Current is generated or induced because tissue contains water and other conductive molecules to allow electrical current to take place in response to the electric fields. Output signals **105** and **107** are electrically processed through said custom circuit board before electrically connecting with conductive segments **225**. The frequency of the alternating polarity of the electric fields largely matches that of the frequency of the alternating currents created thereby. Alternately, outputs **105** and **107** may be electrically connected to the primary inputs on transformer **175**, where secondary outputs of transformer **175** are **105a** and **107a**. Transformer **175** can be used to help stabilize resonance frequency on the target tissue, filter out switching noise from generator **100**, and extend battery life of device **10** by operating generator **100** at more efficient frequency than resonance 460 KHz pertaining to nerve tissue. Further, electrically processed signal from **105**, **105a**, **107**, or **107a** may be looped back to a control unit **125**, as discussed below, where signals are further processed and returned back to inputs **109** and **111** on best mode electric field generator **100**.

Electric field generator **100** is also capable of emitting one or more direct current pulses from **105** or **107** into target tissue **250** in order to provide nerve detection and precise location of high frequency alternating current medical device prior to heat production. Before the surgeon generates the alternating current field that heats target tissue **250**, the surgeon could locate the precise target nerve cell or component thereof using the one or more direct current pulses. Direct current pulses may be of various sizes and shapes where multiple shaped pulses may be emitted from the electric field generator **100** at the same time. The surgeon may position the at least two conductive segments on or into the overall area of the target cell and then emit the pulse or pulses from conductive segments. When one of the pulses is electrically connected to the target nerve cell, the pulse stimulates the muscle that the nerve drives, thereby causing said muscle to twitch or move in some way. Thus, a step of searching for the exact target cell and then a step of final positioning of **200** and **225** may be used to improve precision and accuracy of the surgery to yield the desired precise cell injury. Searching occurs until the sought after muscle twitches or otherwise the correct movement is witnessed, at which point the surgeon knows the correct nerve cell or component thereof has been located and that the at least two conductive segments are now precisely located on the exact target tissue **250**. Thus, high

frequency alternating current medical device **10** can be very precise and accurate because the at least two conductive segments are known to be exactly located correctly by detecting and identifying the precise location of high frequency alternating current delivery to achieve ablation of nerve tissue. At this point, the surgeon may then actuate the alternating current electrical field to cause exact target tissue heating where no heating is done to any other tissue.

Best mode electric field generator **100** is small and miniaturized so that it may be easily held in one hand by the average adult person. Considerable research and development has been accomplished to achieve an electric field generator **100** in such small size. This is the first hand-held radio frequency generator for use in an electro surgery device. Small size was primarily achieved by significant numbers of prototype and testing cycles aimed at reducing power requirements while still achieving desired precise cell injury. As a result, only a standard 9-volt battery is required to power current best mode electric field generator **100** in order to achieve the desired precise cell injury.

In a basic mode, high frequency alternating current medical device **10** would have two probes or needle-type projections **200** and the electric field generated by **100** would be single phase. A circuit diagram for this mode is depicted in FIG. 1. One probe or needle-type projection **200** would include one segment **225** electrically connected to contact **107** and the other probe or needle-type projection **200** would include the other segment **225** electrically connected to contact **105**. In another basic mode, high frequency alternating current medical device **10** would have one probe or needle-type projection **200** and the electric field generated by **100** would be single phase. A circuit diagram for this mode is depicted in FIG. 1A. The single probe or needle-type projection **200** would include both segments **225**. In more complicated modes, device **10** could have many more projections **200** and thus electric field generator **100** would need to have at least an equal number of signal outputs to utilize the many projections, each electrically connected to one probe or needle-type projection **200**. For instance, each projection could emit one of many phase signals or one of many common signals produced by the generator, leaving possibility for a device **10** with very many probes or needle-type projections **200** to create intricate electric field combinations to help yield very specific desired precise cell injury. Or, device **10** could have many probes or needle-type projections **200** with only two signal outputs **105** and **107**, where **105** and **107** signals are connected to the many projections in alternating fashion, perhaps along a row or arc of projections **200**. Alternating only two signals in this fashion can create a large lesion area along the row or arc from only a one-phase alternating electric field because current is created between each projection **200** in this fashion.

Best mode high frequency alternating current medical device **10** has three needle-type projections arranged in a line. See FIGS. 7 and 8. The center projection **200** is electrically connected to common signal **107** or **107a**, generated by electric field generator **100**. The two outer projections are electrically connected in parallel to a single-phase signal **105** or **105a**, generated by electric field generator **100**. A circuit diagram for best mode is depicted in FIG. 2. In all arrangements and modes, it is the phase signal that passes through the self-limiting conductive material electrical component **150** before entering the target tissue.

At least one probe or needle-type projection **200** may be removably attachable to the rest of high frequency alternating current medical device **10**. Further, there may be a wide range of removably attachable at least one or needle-type projec-

tions **75**, **200** of many different types, sizes, shapes, materials, etc. that are removably attachable to the rest of high frequency alternating current medical device. Thus, the invention includes a series of removably attachable tips **75**, where each tip **75** comprises: at least one needle of projection **200** and at least two conductive segments **225** located thereon, where each is electrically connected to the rest of the device according to circuit diagrams on FIGS. 1-2 when attached onto medical device.

One such removably attachable tip **75** may be another nerve finder with two small pads on the distal end. Two small pads are used to electrically connect the surface of the target tissue to the electric field generator **100**. Thus, the nerve finder tip **75** may be first used to find a nerve where another tip **75** would then be attached to heat the nerve once found.

Best mode removably attachable tip **75** is removably attachable to the distal end of high frequency alternating current medical device **10**. Best mode removably attachable tip **75** is of a general conical shape or cup shape with an opening on the wide end of the cone and a flat call member on the narrow end of the cone to form an overall cup shape, where at least one needle-type projection **200** is attached to the exterior surface of the narrow end of the cone or bottom of cup. The distal end of high frequency alternating current medical device **10**, with tip **75** removed, may also have a general conical shape or cup shape, where device cone is slightly smaller than tip cone. Thus, the concave tapered section of tip **75** may then slide onto the convex tapered section of the device cone, where tip **75** snugly fits onto device cone. Further, there may be a securing mechanism such as a clasp means, snap means, lock means, or similar to hold tip **75** onto the device cone in a very stable and secure fashion, so that surgery can be performed by the surgeon. Said securing mechanism would also have a release means so that removably attachable tip **75** may be removed. Thus, clasp means, snap means, lock means, or similar would have capability of releasing said means to remove tip **75**. For instance with snap means, tip cone may be of a flexible nature to allow finger squeezing to cause deformity in tip cone thereby releasing one or more snap points between tip cone and device cone. Specific attachment means is not critical to patentability. When tip **75** is snapped into place onto device **10**, an electrical connection occurs between at least two conductive segments **225** and generator signals **105** or **105a** and **107** or **107a**. Removably attachable tips **75** may be supplied in a sterile condition and then disposed of after use.

The operating frequency of the pulse width modulation power supply can be adjusted within about five percent using either trimmer input connection **109** or **111**. In best mode, trimmer input connections **109** and **111** are electrically connected to a control module **125**. See FIG. 2. Control module **125** is powered by battery **50** and is electrically connected to electric field generator **100**. Control module **125** includes one or more trimmer resistors or similarly functioning electronic components that are electrically connected to a frequency modulation control switch **127**, which is a setting switch on the control unit **125** used to adjust the frequency of signal **105**. This is manual frequency adjustment.

Control module **125** may also automatically fine-tune and stabilize the frequency of signal generated by **100** by sampling signal **105** and electrically processing it to determine whether the frequency is optimum. Signal and current from **105** is electrically filtered, processed, and analyzed where the result yields a signal input to adjust trimmer input **109** or **111**. Thus, control unit creates a feedback circuit from signal output **105** to trimmer input **109**, which results in automatic fine-tuning and stabilization of output. Control unit **125** uses

special arrangements of common circuit board components to custom design the automatic feedback control circuit design. In the case of more than one output phase signal, a feedback circuit may have to be created for each output phase in order to properly automatically fine-tune and stabilize frequency of all phases. Control unit **125** also determines if current through the target tissue is above a certain maximum preset limit and shuts down its electric field generation when said current goes beyond this limit. This is current cut-off setting **129** where the surgeon or technician may set a maximum current level where the device **10** shuts down its electric field generation above this level.

At least two electrical outputs: phase signal **105** and common signal **107** essentially perform the surgery. Outputs may be filtered, transformed, and otherwise electrically processed through standard circuit board components to yield desired precise cell injury. Phase signal **105** passed through self-limiting conductive material electrical component **150** on to the target tissue **250**. It then travels through the target tissue **250** and back to the electric field generator **100** through common signal **107**. Of course, this is alternating current so it is really back and forth electron motion rather than passing through.

Self-limiting conductive material electrical component **150** regulates electrical current through the target tissue **250**. As stated, self-limiting conductive material electrical component **150** functions electrically like a thermistor, thermocouple, or switch. A thermistor is a type of resistor whose resistance varies with temperature of itself. A thermocouple is an electrical component that produces a voltage that varies with its temperature and is widely used to control temperature. A switch is an electrical component that can break an electrical circuit by interrupting the current in the circuit. In all cases, self-limiting conductive material electrical component **150** regulates electrical current through the target tissue **250** as a function of its temperature.

If the case of self-limiting conductive material electrical component **150** being a switch, the alternating current in the target tissue is completely shut down by **150** for a brief period of time until the target tissue has sufficiently cooled, thereby avoiding unnecessary cell damage, and then switch **150** would switch the alternating current in the target tissue back on again, thereby heating it up again, for a brief period, only to turn off again, repeating the process. This process essentially repeats many times per second yielding an overall steady state temperature in the target tissue.

If the case of self-limiting conductive material electrical component **150** acting like a thermistor or thermocouple, the temperature changes of **150** do not lead to an abrupt off/on switching of alternating current in the target tissue, but rather yield a gradual heat increase or decrease as described below to control temperature of the target tissue and surrounding tissue. Thermistor has the most gradual fluctuations of alternating current.

Self-limiting conductive material electrical component **150** consists essentially of a homogeneous blend of different materials, including a base material and a conductor dopant. Self-limiting conductive material electrical component **150** has a special combination of base and dopant that allows the resistance of a self-limiting conductive material electrical component to vary with its temperature. As current passes through the self-limiting conductive material electrical component **150**, heat is produced in the self-limiting conductive material electrical component **150** as a result of electron, ion, or other charged-particle collisions occurring inside **150** as a result of the alternating current is passing through target tissue **250**. Thus, increased current through target tissue **250**

yields increased heat production in self-limiting conductive material electrical component **150**. This heat causes structural changes in the molecules of the homogeneous blend of material, which in turn causes a change in conductivity of self-limiting conductive material electrical component. For instance with some self-limiting conductive materials or thermistors, heat causes the base material to expand, which separates a conductive dopant suspended therein, thereby reducing, and eventual cutting off, the electrical current passing there through. In other self-limiting conductive materials or thermistors, temperature change causes a phase change of base or dopant material, which causes structural changes at the molecular level yielding a switching effect from conductive to nonconductive or vice versa.

Thermistors, thermocouples, and switches of this sort may be custom designed with a specific recipe of self-limiting conductive material to yield a specific temperature/resistance relationship and thus a specific temperature range of target area. If resistance increases with increasing temperature, the material may be called a positive temperature coefficient (PTC) thermistor or posistor. If resistance decreases with increasing temperature, the material may be called a negative temperature coefficient (NTC) thermistor. Standard resistors are designed to have constant resistance over a wide temperature range and are sometimes called zero temperature coefficient (ZTC) materials, which could be another subset of thermistor. There are many commercially available self-limiting conductive materials or thermistors that have various temperature/conductivity properties. Custom temperature/conductivity characteristics and sizes are also commercially available.

At any rate, very special care must be taken to choose/design the best self-limiting conductive material electrical component **150** to yield the best mathematical characteristics between temperature and resistance, to yield to best surgical performance, i.e. the required temperature range to cause the desired precise cell injury. The relationship between temperature and conductivity of a self-limiting conductive material electrical component is typically nonlinear, so we use log scales to describe thermistor properties. Conductivity is typically measured by the inverse of such which is resistivity.

In best mode, self-limiting conductive material electrical component **150** is made of PTC material. FIG. 3 is a graph of the electrical resistivity versus temperature of a PTC heater material suitable for our purposes. Suitability for typical procedures requires a resistivity that gradually increases with temperature as noted by the mid-level positive slope character of the graph. Further, there is an inflection point in the graph at  $T_0$ . As temperature rises above  $T_0$ , resistivity increases at a decreasing rate with temperature. Thus, there is a gentle decrease at a decreasing rate of electrical current passing through the target tissue as temperature rises above  $T_0$ . As temperature falls below  $T_0$ , resistivity decreases at a decreasing rate with temperature. Thus, there is a gentle increase at a decreasing rate of electrical current passing through the target tissue as temperature falls below  $T_0$ . With reference to FIG. 3, going from  $T_0$  to  $T_H$ , resistivity gradually increases, thereby decreasing heat production in the target tissue. Likewise, going from  $T_0$  to  $T_L$ , resistivity gradually decreases, thereby increasing heat production in the target tissue. There is a mathematically stable temperature point at  $T_0$ , otherwise known as an inflection point. Materials with this inflection point relationship yield perfect characteristics for best mode because this yields optimal stability to keep the self-limiting conductive material electrical component very steadily set at  $T_0$ , thereby producing a steady alternating current in the target area.



The temperature of the self-limiting conductive material electrical component **150** determines the electrical current passing through the target area. Thus, the key design criteria of the high frequency alternating current medical device **10** is the determination of what minimum electrical current is required to produce the desired precise cell injury, then what self-limiting conductive material electrical component provides this quantity of current at it mathematical equilibrium, thereby determining the best self-limiting conductive material electrical component for the application of the high frequency alternating current medical device.

Different precise cell injury procedures may require different cell heating or electrical current operating ranges. For instance, different procedures may require different shaped and sized probes of needle-type projections **200**, thereby changing current requirements, thereby changing the self-limiting conductive material electrical component requirements of the high frequency alternating current medical device **10**. Different target tissues may require different current or heating thereby doing the same. Thus, certain procedures may require different self-limiting conductive material electrical component with different target temperatures  $T_0$  with different operating ranges  $T_H$  to  $T_L$ . These criteria may be adjusted by carefully choosing a PTC, NTC, or ZTC thermistor material for the high frequency alternating current medical device **10**. Further, various dopants and various concentration of dopants may be used to vary characteristics to yield different resistance temperature graphs. Further combinations of PTC, NTC, and ZTC materials may be used to yield different resistance temperature graphs.

FIG. 4A includes the resistance temperature relationship of a NTC material. This arrangement may be used to create a maximum operating current as determined by temperature  $T_0$  with sharp cut-off at currents above such. FIG. 4B includes the resistance temperature relationship of a ZTC material. This arrangement may be used to create constant current across the target area at a certain level across a wide range of temperatures  $T_H$  to  $T_L$ . FIG. 4C includes the resistance temperature relationship of a NTC/ZTC material. This arrangement may be used to create a wide operating current range correlated to that of  $T_H$  to  $T_L$  with constant current at a certain level but with sharp cut-off at temperature  $T_L$ . FIG. 4D includes the resistance temperature relationship of a PTC/ZTC material. This arrangement may be used to create a wide operating current range correlated to that of  $T_H$  to  $T_L$  with constant current at a certain level but with sharp increase in current at temperature  $T_L$  thereby preventing the target tissue a certain temperature.

PTC, NTC, and ZTC materials can be made from a crystalline or semi-crystalline polymer base material with certain conductive "doping" material added. With polymer based thermistors, transition temperature results from the melting or freezing of polymer molecules. With crystalline or semi-crystalline polymers, molecular structure is more tightly packed in solid phase and less tightly packed in amorphous phase or elastomer phase. Polymer molecules are generally non-conductive, so a conductive dopant must be added to make the material conductive. At temperatures below  $T_0$ , most polymer molecules are in solid phase, thus closely packed, thus at their most conductive state or level. At temperatures above  $T_0$ , most polymer molecules are in amorphous phase or elastomer phase, thus loosely packed, thus at their least conductive state or level. For the same choice of a matrix polymer, transition temperatures  $T_0$  generally coincide with the polymer softening point of the selected matrix polymer.

Dopant material is added to base material in order to render it conductive which allows the material to perform like a heating element. Also dopant is added to slow the resistance change or to widen the graph discussed above. Dopants are conductive material such as carbon black, metal oxide, semiconductor material, blends thereof, or other material that is conductive and capable of being produced in small particles. The specific resistivity temperature relationships of PTC, NTC, and ZTC materials are arrived at by varying the type and concentration of dopant. Thus, a lower concentration or density of conductive particles in the polymer base composition is one way to obtain the desired gradual change in resistance for a self-limiting heater element. Generally speaking, dopant levels above 50 percent yield switch type material, dopant levels of 15-40% yield thermistor material, and dopant levels of 10% yield electro magnetic interference and or electrostatic discharge. Also, porosity, surface area, particle size, and oxygen content, of the conductive dopant may be varied to produce various properties. Also, more than one type of dopant may be added to base material. Either the base material molecules or the dopant material particles may actually cause the heating in the thermistor. Thus, dopant may function to produce electron transfer or vibrational heating or both. All of these factors together with various carbon black loading levels and others results in a near endless amount of combinations between type(s) and amount(s) of dopant along with type(s) of base material to yield a near endless amount of specific resistivity temperature relationships.

PTC, NTC, and ZTC materials can also be made from a ceramic material or ceramic based material with conductive dopant added. Ceramic material can be conductive or not conductive depending on phase or structure. Ceramic material can be engineered to change phase from solid to elastomer or elastomer to solid at specific temperatures  $T_0$ . Typically, ceramic base material is barium titanate and/or related divalent titanates and zirconates. Typical dopants include lead, strontium, rare earth metals, antimony, bismuth, or similar. Dopants are added to increase or decrease the anomaly range of the base material or further adjust the slope of the resistivity temperature relationship. Various ceramic thermistor heaters with different temperature resistivity relationships are commercially available. Also, a ceramic thermistor heater material manufacturer may endeavor to undertake special development programs to deliver specially desired characteristics.

In some modes, traditional switches are added to the tissue heating circuit or circuits or traditional thermocouples are placed near conductive segments **225** or both to further enhance temperature control of target tissue **250** or to add additional layers of safety current cut-off control or similar during electric field generation mode or surgical mode.

High frequency alternating current medical device **10** typically includes a user interface **20** comprising a main power on/off switch **21**, an electric field on/off switch **23**, a main power indicator light **25**, and an electric field indicator light **27**. User interface **20** is electrically connected to control module **125**, sending and receiving signals there from, and is indirectly powered by battery **50** through control module **125** electrical connections. Main power switch **21** engages power to electric field generator inputs and to control module **125**. When switch **21** is on, power indicator light **25** is illuminated. Surgery may be performed when the electric fields are generated, which is controlled by the electric field on/off switch **23**. When switch **23** is activated, the electric field is engaged between the at least one probe or needle-type projection **200**. Electric field indicator light **27** illuminates when electric field on/off switch **23** in engaged.

As stated, best mode high frequency alternating current medical device **10** is a hand-held battery powered single device. To facilitate this, all components are assembled onto one small circuit board. In this configuration, switches **21** and **23** may be located on the exterior of high frequency alternating current medical device **10** and at a location in close proximity to the index finger of the surgeon holding high frequency alternating current medical device **10**. Lights **25** and **27** may also be located on the exterior of high frequency alternating current medical device **10**. Frequency modulation setting **111** and cut-off setting **113** may be located in the interior of device **10** because they are typically set differently for certain procedures and do not need to be adjusted during the procedure.

In order to yield the most comfortably and logical instrument for a surgeon, best mode high frequency alternating current medical device **10** is shaped like a pen. The delicate nature of producing a desired precise cell injury requires fine hand movements similar to that of writing in very small print. Thus, the surgeon that is comfortable writing with a pen is also comfortable using high frequency alternating current medical device **10** to yield desired precise cell injury.

Best mode at least one probe or needle-type projection **200** has a diameter of 0.5 to 7 millimeters in outer diameter and length of 5 millimeters and up with a piercing distal end. Best mode at least one probe or needle-type projection **200** primarily has a non-conductive surface that is not electrically connected to signal outputs **105** or **107** and thus does not emit an electric field except for at certain segments **225** of the probe or needle-type projection **200**. Only at segments **225** will an electric field emit there from. As stated, at least two conductive segments **225** are required to generate electrical current in target tissue. In the most two basic modes of high frequency alternating current medical device **10**, at least two conductive segments **225** are both located on one probe or needle-type projection **200** or one segment **225** is located on each of two needle-type projections **200**. Conductive segments **225** may have a layer or coating or alternately may not have a layer or coating that causes segments **225** to be conductive. For instance, the needles may be made of nonconductive material where conductive segments are formed by one or more conductive coatings thereon. Needles may be made of conductive material with nonconductive coatings on the surface except at conductive segments **225**. Any assembly of conductive and nonconductive materials may be used to yield needles/probes with effective conductive segments **225**. Segments **225** are electrically connected to signals **105** or **107**. When segments **225** are located on the distal ends of probes or needle-type projections **200**, heat is produced below the surface of the tissue only, thereby providing much more opportunity to cause the desired precise cell injury without also changing the surface of the tissue. In best mode, segments **225** are located at the distal ends of needle-type projections **200** and are about 1-4 millimeters in length.

The method of using said high frequency alternating current medical device **10** comprises the steps of: picking up said high frequency alternating current medical device **10**, turning on said high frequency alternating current medical device, touching said at least one probe or needle-type projection **200** to the surface of target tissue **250**, inserting said at least one probe or needle-type projection **200** beneath the surface of target tissue **250**, or inserting said at least one probe or needle-type projection **200** into a body cavity **250**, engaging said electric field generator **100** thereby inducing or generating an electrical alternating current in target tissue **250**, disengaging the electric field generator **100**, removing said at least one probe or needle-type projection **200** from said target tissue

**250**, and repeating the former steps as necessary to cause the desired certain desired precise cell injury.

A high frequency alternating current medical device constructed according to the present invention may be used by touching at least one probe or needle-type projection **200** to target tissue **250**, whether on the skin surface of a patient, subcutaneously or deeper. If the target tissue is skin or subcutaneous tissue, a specific type of probe and temperature may be chosen to achieve skin tightening, resurfacing or collagen remodeling. The maintenance temperature of the device could be chosen to be not more than 41° C. (106° F.). At such a moderate temperature **200** can produce skin tightening, skin resurfacing and collagen remodeling, for dermal regeneration and cosmetic applications. This can also be accompanied by mechanical ablation of skin surface cells. Alternatively, a higher temperature could be used to cut skin, while simultaneously cauterizing any bleeding.

If the target tissue is subcutaneous adipose (fat) tissue, **200** must have piercing structure to be inserted into the skin to cause selective damage to fat cells proximate to the end of **200**.

The target tissue might be glandular, as in sweat glands of the skin to treat hyperhidrosis or the tonsils in the oral cavity in performing a total or partial tonsillectomy.

The target tissue could be vascular (veins, arteries, capillaries, blood), wherein heat transfer through the probe can be used to produce local blood coagulation and cauterization of the vascular tissue. Or, at more gentle temperatures (near 37° C. body temperature), a hollow probe can inject a pre-heated fluid into the target artery or vein, e.g., for localized drug delivery.

The target tissue could be some abnormal growth, polyp or tumor, such as in the sinus or oral cavity. Here, heat transfer through the probe can ablate that tissue. Examples include: mucosal lesions found in Barrett's esophagitis, or tissue growth from nasal turbinate hypertrophy, or removal of colon or rectal polyps.

The target tissue might be any organ system in the body, such as heart, lungs, brain, eyes, kidney, liver, ovaries, thyroid, bladder, uterus, stomach, intestines, appendix, gall bladder, or similar.

What is claimed is:

1. A high frequency alternating current medical device comprising:
  - an electrical power source;
  - an electric field generator;
  - a self-limiting conductive material electrical component;
  - at least one probe or needle-type projection; and
  - at least two conductive segments, wherein,
    - said at least one probe or needle-type projection is located at the distal end of said high frequency alternating current medical device and is capable of being inserted to tissue or a body cavity,
    - said at least two conductive segments are located on said at least one probe or needle-type projection,
    - said at least two conductive segments are capable of electrically connecting to an electrically conductive foreign medium in contact with said at least one probe or needle-type projection,
    - said at least two conductive segments are electrically connected to said electric field generator, said electric field generator is electrically connected to said electrical power source,
    - said electric field generator is capable of producing at least one phase signal wave output and at least one common signal wave output,

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said at least one phase signal wave output is electrically connected to one or more said at least two conductive segments and said at least one common signal wave output is electrically connected to one or more said at least two conductive segments, such that each of said at least two conductive segments is electrically connected to either a phase signal wave output and a common signal wave output,

said at least one phase signal wave output and at least one common signal wave output are capable of producing an alternating polarity electric field between said at least two conductive segments, wherein said alternating polarity electric field may induce an electrical alternating current between said at least two conductive segments when contacted by electrically conductive outside material such as human or animal tissue, said self-limiting conductive material electrical component is placed in electrical series connection between said electric field generator and said at least one phase signal output, and

said self-limiting conductive material electrical component consists primarily of: a polymer base material with 5-40% conductive dopant material, a ceramic base material with 1-40% conductive dopant material, or a ceramic material without dopant material, wherein, said self-limiting conductive material electrical component is characterized by an electrical resistance that varies with temperature.

2. The high frequency alternating current medical device as recited in claim 1, wherein said electrical power source is a direct current battery of any voltage or an alternating current power source of any voltage.

3. The high frequency alternating current medical device as recited in claim 1, wherein said a self-limiting conductive material electrical component is made primarily of: positive temperature coefficient material; negative temperature coefficient material; zero temperature coefficient material; a combination of zero temperature coefficient material and negative temperature coefficient material; or a combination of zero temperature coefficient material and positive temperature coefficient material.

4. The high frequency alternating current medical device as recited in claim 3, wherein said self-limiting conductive material electrical component is a thermistor, thermocouple, or switch.

5. The high frequency alternating current medical device as recited in claim 4, wherein all components of said high frequency alternating current medical device are assembled inside a small handheld enclosure.

6. The high frequency alternating current medical device as recited in claim 5, wherein said small handheld enclosure is oblong-shaped.

7. A high frequency alternating current medical device as recited in claim 6, wherein said small handheld enclosure has exterior surfaces shaped like a pen or a mechanical pencil or marker.

8. The high frequency alternating current medical device as recited in claim 5 with two probes or needle-type projections and two conductive segment where each probe or needle-type projection has one conductive segment located thereon.

9. The high frequency alternating current medical device as recited in claim 5 with three probes or needle-type projections and three conductive segments where each probe or needle-type projection has one conductive segment located thereon.

10. The high frequency alternating current medical device as recited in claim 1, wherein said at least one probe or needle-type projection and at least two conductive segments

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located thereon are removably attachable to the rest of said high frequency alternating current medical device wherein said at least one probe or needle-type projection can be attached and locked into place, electrically connecting said at least two conductive segments to said at least one phase signal wave output or said at least one common signal wave output to that surgery may be performed, and then unlocked and removed from said high frequency alternating current medical device.

11. The high frequency alternating current medical device as recited in claim 1, wherein at least one probe or needle-type projection is needle-shaped with an outside diameter of 0.5 to 7 millimeters.

12. The high frequency alternating current medical device as recited in claim 1, wherein at least one probe or needle-type projection has cross-sectional shape that is circular, oval, square, rectangular, or oblong.

13. The high frequency alternating current medical device as recited in claim 1, wherein at least one probe or needle-type projection has a distal end that is: rounded, roller-balled, piercing, pointed, or blunt.

14. A method of using a high frequency alternating current medical device comprising:

- a) obtaining a high frequency alternating current medical device having at least one probe or needle-type projection with at least two conductive segments;
- b) switching on said high frequency alternating current medical device, including electrically coupling a electrical power supply to a electric field generator;
- c) touching a distal end of said at least one probe or needle-type projection to a surface of a target tissue, inserting the distal end of said at least one probe or needle-type projection beneath the surface of the target tissue, or inserting the distal end of said at least one probe or needle-type projection into a body cavity containing a target tissue;
- e) switching on said electric field generator, including electrically coupling each of said at least two conductive segments to at least one of a phase signal wave output and a common signal wave output, thereby generating an alternating polarity electric field between said at least two conductive segments;
- f) switching off said electric field generator, including electrically decoupling each of said at least two conductive segments from said electric field generator;
- g) adjusting or repositioning the distal end of said at least one probe or needle-type projection on or in said target tissue;
- h) switching on said electric field generator, including electrically coupling each of said at least two conductive segments to said electric field generator to either said at least one phase signal wave output or said at least one common signal wave output, thereby generating an alternating polarity electric field between said at least two conductive segments;
- i) switching off said electric field generator, including electrically decoupling each of said at least two conductive segments from said electric field generator;
- j) repeating steps g through i until a desired precise cell injury is attained; and
- k) removing the distal end of said at least one probe or needle-type projection from said target tissue.

15. The method of claim 14 further comprising the following steps inserted after step (a):

- removing said at least one probe or needle-type projections with said at least two conductive segments located thereon from the rest of said high frequency alternating

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current medical device, wherein said at least one probe or needle-type projections with said at least two conductive segments located thereon is removably attachable to the rest of said high frequency alternating current medical device;

choosing from a set of said at least one probe or needle-type projections with said at least two conductive segments located thereon, wherein each of said set has a different shaped said at least one probe or needle-type projections that may be appropriate for a certain type or size of target cell and certain type of desired precise cell injury;

attaching said chosen at least one probe or needle-type projections with said at least two conductive segments located thereon to the rest of said high frequency alternating current medical device using an attachment means that is reversible and lockable so that when attached said at least one probe or needle-type projection is solidly connected to the rest of said high frequency alternating current medical device and required electrical connections are completed so that surgery may be performed; and

completing steps (b) through (k).

16. The method of claim 14 or 15, wherein said step of touching the distal end of at least one probe or needle-type projection to a target tissue, piercing the distal end of at least one probe or needle-type projection into a target tissue, or inserting the distal end of at least one probe or needle-type projection into a body cavity containing a target tissue forms part of a pain management or treatment protocol.

17. The method of claim 14 or 15, wherein said target tissue is skin and said desired precise cell injury is skin tightening, skin resurfacing, collagen remodeling, tissue cutting, tissue ablation, or pain relief.

18. The method of claim 14 or 15, wherein said target tissue is subcutaneous adipose tissue and said desired precise cell

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injury is selective damage to fat cells proximate to said at least one probe or needle-type projection.

19. The method of claim 14 or 15, wherein said target tissue is nerve tissue and said desired precise cell injury is ablation of nerve tissue yielding wrinkle relaxation, pain relief, muscle twitch or spasm relief, or repair of cardiac electrical conduction abnormalities.

20. The method of claim 14 or 15, wherein said target tissue is a rami of the temporal branch of the facial nerve or the angular nerve supplying innervations to the corrugator and procerus muscles of the face.

21. The method of claim 14 or 15, wherein said target tissue is glandular including sweat glands of the skin or tonsils of the oral cavity.

22. The method of claim 14 or 15, wherein said target tissue is vascular tissue and said desired precise cell injury is blood coagulation and cauterization of the vascular tissue or ablation or shrinkage of atherosclerotic plaques in blood vessels.

23. The method of claim 14 or 15, wherein said target tissue is polyp, tumor, lesion, or abnormal growth and said desired precise cell injury is ablation said target tissue.

24. The method claim 14 or 15, wherein said target tissue is selected from the group consisting of epidermis skin, dermis skin, mucosal lining, cartilage, muscle, bone, tendons, ligaments, central nervous system, brain, spine, peripheral nervous system, heart, liver, stomach, kidney, bladder, prostate, lungs, intestines, gallbladder, appendix, spleen, brain, tongue, orbits, ocular tissue, auditory system, teeth, tonsils, adenoids, salivary glands, uterus, ovaries, testicular tissue, nasal or sinus tissue, thyroid, parathyroids, pancreas, adrenal glands, pharynx, larynx, esophagus, rectum, lymphatic tissue, and vascular tissue.

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